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UNDERSTANDING THE BIOMECHANICS OF MEDIAL TIBIAL STRESS SYNDROME
– A SIMULATION STUDY USING A MUSCULOSKELETAL MODEL

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INTRODUCTION
Foot pronation is a complex triplanar movement. Visually, it is characterized by a flattening of the Medial Longitudinal Arch (MLA) and an abduction of the calcaneus. The diagnosis Medial Tibial Stress Syndrome (MTSS) has been associated with a greater degree of foot pronation. O’Connor et al. [1] suggested that passive properties may primarily account for the increased energy absorption associated with greater foot pronation. Bouche et al. [2] have hypothesized that large foot pronation induces tension on the tibial fascia at its insertion into the medial tibial crest and this could be one of the causes of MTSS. Due to the highly complicated and invasive nature of experimental investigations of this problem, the current study suggests an analytical approach for understanding the biomechanics of the lower leg and excessive pronation of the foot.

METHODS
A musculoskeletal model of the lower extremity was built in the AnyBody Modeling System [3]. The model was based on cadaver data [4] and included 38 muscles that were divided into 316 muscle fascicles, based on the line-of-action. A Hill-type muscle model with passive elasticity and force-length-velocity relationships was used. The model was driven through a gait cycle with kinematic and kinetic data from a gait experiment on a healthy male (173 cm; 85 kg). For simulating different degrees of pronation, the right foot was artificially rotated about an axis (Figure 1) going from the calcaneus and through the 2nd metatarsal bone. The rotation went from 20˚ pronation to -5˚ supination, mimicking foot postures from highly pronated to slightly supinated. The simulations were run with increments of 5˚. For each foot posture the muscle recruitment problem was solved and the passive force of the muscles in the deep flexor compartment was estimated.

RESULTS AND DISCUSSION
When the degree of pronation is increased the m. tibialis posterior has less activity, especially between the heel strike and stance phase (Figure 2). The passive elastic forces from the muscles included in the deep flexor compartment increased as the pronation became more excessive. Figure 2 shows the passive elastic forces in the muscles as a function of the stance phase.

CONCLUSIONS
Based on the results found from the simulations, it can be concluded that the musculoskeletal model supports the theory suggested by Bouche et al. [2].

REFERENCES