



# The nociceptive withdrawal reflex in conscious dogs

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# The nociceptive withdrawal reflex in conscious dogs: a new, non-invasive model of nociception

Ph.D. thesis

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2008

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To my parents, with love.

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# 1. Abbreviations

NWR: nociceptive withdrawal reflex It: individual NWR threshold intensity TSt: temporal summation threshold intensity RMS: root-mean-square EMG: electromyography ACP: acepromazine SAL: saline ms: milliseconds NMDA : N-methyl-D-aspartate WDR: wide dynamic range CRI : constant rate infusion IV: Intravenous IQR : inter quartile range AUC : area-under-the-curve

# 2. Acknowledgments

The present studies have been carried out at the Anaesthesiology division, Department of Clinical veterinary medicine, Vetsuisse Faculty, University of Berne and at Novartis Pharma, Basel, Switzerland.

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Berne, 06 08 2008

# 3. List of original publications

The present thesis is based on the following original publications, referred to in the text by their Roman numerals (I- IV).

I. <u>Alessandra Bergadano</u>, Ole K. Andersen, Lars Arendt-Nielsen, Urs Schatzmann, Claudia Spadavecchia. Quantitative assessment of nociceptive processes in conscious dogs by use of the nociceptive withdrawal reflex. AJVR 2006; 67;5:882-9 doi: 10.2460/ajvr.67.5.882

II. <u>Alessandra Bergadano</u>, Ole K. Andersen, Lars Arendt-Nielsen, Claudia Spadavecchia. Non invasive assessment of the facilitation of the nociceptive withdrawal reflex by repeated electrical stimulations in conscious dogs. AJVR 2007; 68;8:899-907 doi: 10.2460/ajvr.68.8.899

III. <u>Alessandra Bergadano</u>, Ole K. Andersen, Lars Arendt-Nielsen, Claudia Spadavecchia. Modulation of a low acepromazine dose on single and repeated nociceptive stimuli in conscious dogs. VAA 2008 (Accepted)

IV. <u>Alessandra Bergadano</u>, Ole K. Andersen, Lars Arendt-Nielsen, Regula Theurillat, Wolfgang Thormann, Claudia Spadavecchia. The plasma concentrations of a low-dose constant-rate-infusion (CRI) of ketamine and its effect on single and repeated nociceptive stimuli in conscious dogs. Vet J 2008 (In press) doi:10.1016/j.tvjl.2008.06.003

# 4. Abstract (English)

In this thesis the nociceptive withdrawal reflex (NWR) and its facilitation by repeated electrical stimulations in intact, conscious dogs were thoroughly investigated. This included methodological development and pharmacological modulation studies. The pharmacological modulation aimed to quantify objectively the efficacy of different drugs in dogs.

In paper I the feasibility of evoking and recording the NWR from the forelimb and hind limb of conscious non-medicated dogs was first described. The stimulus-response curves and the evoked behavioral responses were studied confirming the nociceptive origin of the reflex. In paper II, the facilitation of the nociceptive withdrawal reflex by repeated electrical stimuli as a measure of neuronal temporal summation and the associated behavioral response scores were investigated in conscious, non-medicated dogs. Additionally the influence of stimulus intensity and stimulus frequency on temporal summation responses were analyzed. In paper III, the within-session and intersession stability of the NWR thresholds could be demonstrated, supporting that the model is reproducible and robust. Furthermore it was shown that intravenous 0.01 mg kg<sup>-1</sup> acepromazine can be used to ease data acquisition in anxious subjects without altering the validity of the model. Based on these findings, the antinociceptive action of a low-dose constant-rate-infusion of racemic ketamine (0.5 mg kg<sup>-1</sup> loading bolus followed by 10  $\mu$ g kg<sup>-1</sup> min<sup>-1</sup>) in conscious dogs was explored in paper IV. Temporal summation and the evoked behavioral responses scores were inhibited compared to baseline, demonstrating the antinociceptive activity of ketamine in correlated with peak plasma concentrations. This antinociceptive action was short lived owing to the unexpectedly low plasma levels obtained at pseudo-steady-state, questioning the use of this low-dose ketamine CRI as sole analgesic in dogs.

In conclusion the work presented in this PhD thesis has provided a new, non invasive, robust experimental model of nociception in conscious dogs that may be used in clinical routine to study the antinociceptive activity of drugs or to quantify the excitability of the nervous system in individual canine patients.

# 5. Abstract (Danish)

I denne afhandling beskrives den nociceptive afværgerefleks (NWR) og dens facilitering ved hjælp af gentagne elektriske stimulationer på intakte hunde, der er ved fuld bevidsthed ("intact" på engelsk henviser typisk til ikke kastreret/steriliseret). Dette indebar metodeudvikling og farmakologiske modulationsundersøgelser. Den farmakologiske modulation havde til formål objektivt at kvantificere effekten af forskellig medicin i hunde.

I den første artikel beskrives anvendeligheden af en metode til at fremkalde og registrere NRW fra forog bagben på vågne, ikke medicinerede hunde. Stimulus-responskurven og den fremkaldte adfærdsrespons bekræftede den nociceptive oprindelse af refleksen.

I den anden artikel beskrives undersøgelsen af faciliteringen af NWR ved hjælp af gentagne elektriske stimuli som et mål for neuronal temporal summation og de tilhørende adfærdsrespons-scores i vågne, ikke medicinerede hunde. Desuden blev indflydelsen af stimulus-intensiteten og stimulus-frekvensen på temporal summations-responsen analyseret.

I tredje artikel kunne winhin-session og intersession stabiliteten af NWR'ens grænseværdier demonstreres, hvilket understøtter modellens stabilitet og reproducerbarhed. Desuden blev det påvist, at intravenøs acepromacin i en dosis på 0,01mg per kg kan bruges på meget nervøse hunde for at lette erhvervelsen af data, uden at det har indflydelse på modellens validitet.

Baseret på de ovennævnte resultater blev den antinociceptive virkning af en konstant lav-dosis infusion af racemic ketamin (0,5 mg kg<sup>-1</sup> som start-bolus efterfulgt af 10  $\mu$ g kg<sup>-1</sup> min<sup>-1</sup> konstant infusion) undersøgt i fjerde artikel. Temporal summation og de fremkaldte adfærdsrespons-scores blev hæmmet sammenlignet med basislinien. Dette demonstrerede den antinociceptive virkning af ketamin i korrelation med peak plasma-koncentrationer. Denne antinociceptive virkning var kortvarig på grund af de uventede lave plasma-koncentrationer opnået på pseudo-steady state. Dette sætter spørgsmålstegn ved brugen af denne lav-dosis ketamin-infusion som eneste analgetiske medicin hos hunde.

Afsluttende kan man sige, at det arbejde, der præsenteres i denne Ph.d.-afhandling har leveret en ny, ikke-invasiv, solid eksperimentel model for nociception i hunde ved bevidsthed, der kan bruges i klinisk rutine-arbejde til undersøgelse af den antinociceptive virkning af medikamenter eller til at kvantificere excitabiliteten af nervesystemet i individuelle hunde.

# 6. Introduction

Understanding and treating pain in animals is one of the most challenging tasks in veterinary medicine. In the last decade there has been a growing interest and research investigating the mechanisms underlying animal pain and improving the therapeutic options (Hansen 2003). In 2002, experts in animal and human pain developed a consensus statement indicating that animals feel pain and identified the key gaps in the current knowledge of animal pain (Paul-Murphy et al. 2005). Because animals lack the ability to use language to express emotions about pain, animal pain has been described in terms of behavioural responses to damaging or potentially damaging noxious stimuli. The term "nociception" (i.e. perception of a damaging or potentially damaging stimulus) is therefore used, also for the purpose of this thesis, as it thought to represent more accurately the response to stimuli which would be associated with pain in man.

To date the most important gap in our knowledge of animal pain is related to the assessment of nociception. Subjective assessment of abnormal demeanour or behaviours are extensively used and multiple scales and scoring system have been developed in the attempt to better diagnose and quantify pain. However, there is currently no gold standard to assess nociception in animals and no unit for pain. And as stated by Lord Kelvin many years ago "when you can measure what you are speaking about and express it in numbers you know something about it; but when you cannot measure it, when you cannot express it in numbers, your knowledge is of a meagre and unsatisfactory kind" (Kelvin 1891). It is difficult to say that pain have been effectively if it cannot be accurately assessed.

Another gap is related to a paucity of species-specific information concerning both basic nociceptive mechanisms and efficacy of analgesics. Many current treatments are still extrapolated across species and from experimental to clinical setting without any evidence of their efficacy or safety in a given animal species.

To fill these gaps, there is a substantial need for a noninvasive, sensitive, specific, repeatable model to investigate nociception for basic physiological studies, to objectively assess the degree of sensory dysfunction and to quantitatively test pharmacological interventions. The final goal is to improve the clinical treatment of pain in domestic animals.

# 6.1. Pain in dog and its diagnose

Dogs can experience physiological or pathological pain of inflammatory (somatic or visceral), neuropathic or mixed origin. Many health conditions, medical and surgical procedures cause pain in dogs, mainly of short duration (< 7 days) (Muir et al. 2004). The assessment of pain relies on the subjective description of abnormal behavior and demeanor patterns, or on the use of Visual Analogue Scales after direct or video-assisted (Hansen 2003) observation of the animal. To improve objective and quantitative assessment of nociception, composite pain scales incorporating behavioral, physiological and interactive parameters have been developed (Holton et al. 1998; Holton et al. 2001). Still few have been validated

and only for a specific noxious stimulus. These scales are not valid for assessing pain of another origin: i.e. if a pain scale has been developed to evaluate acute postoperative pain after orthopedic surgery it will not be sensitive for assessing abdominal pain.

The issue of pathological pain in dogs is even more complex. Only very recently there is increased consciousness that dogs of any age can suffer of chronic pain. The most common medical conditions are chronic musculoskeletal pathologies, i.e. hip dysplasia, cruciated ligament rupture, osteoarthritis (Jauernig et al. 1999), and cancers (Lascelles & Main 2002). Chronic pain impairs the quality of life of the animals, and represents a source of practical problems for the owners. Both veterinarians and owners are convinced that those dogs should receive adequate pain-relieving treatment. However, accurate detection of signs of pain and therefore adequate therapy is difficult. In dogs, few very scales are reported to be valid for evaluating chronic osteoarthritis-associated pain (Bjorkman et al. 1993; Wiseman-Orr et al. 2004; Cimino Brown et al. 2007) and other types of chronic pain are actually not addressed. To date pathological pain conditions in dogs are still under-recognized and thus under-treated.

# 6.1.1. Nociceptive models in dogs

Investigations involving animal models of nociception (Le Bars et al. 2001) are mainly used as transitional studies to provide better understanding of pain mechanisms and the effectiveness of analgesic drugs for subsequent administration to humans. Unlike cats (for which there is extensive literature), dogs are seldom used as experimental animals in nociception studies. Some experimental and clinical studies have been performed in dogs to provide objective ways of assessing antinociceptive activity of analgesics for the benefit of the dogs. Mechanical, (Hamlin et al. 1988; Barnhart et al. 2000a; Barnhart et al. 2000b) thermal (Andrews & Workman 1941; Ylisela & Vainio 1989; Barnhart et al. 2000b; Wegner et al. 2008), and electrical stimulations (Hamlin et al. 1988; Vainio et al. 1989; Brown et al. 2002b; Brown et al. 2002a) have been applied to the skin to evoke nocifensive reactions and to evaluate their pharmacologic modulation. The end point of these models of acute nociception in dogs is determined by monitoring the evoked gross behavioral reaction or the thresholds at which the behavioral aversive response is elicited. The prolongation of the latency of the withdrawal response or an increase in the response threshold is interpreted as antinociception.

The major drawback of all these models is evident when the drugs used exert a contemporaneous sedative effect that can clearly alter the pattern of the behavioral reaction observed and the interpretation of the antinociceptive efficacy. Another drawback is that the stimulus intensities used are supramaximal with obvious distress for the animals and potential risk of tissue damage. Additionally these models are modestly sensitive as they do not allow analysing the stimulus-response curve.

A more refined model consists of recording the behavioral reflex response to a nociceptive (thermal or electrical) stimulus by electromyography. Reflex-evoked muscle action potentials of the masseter muscles

after sensory dental pulp stimulation have been recorded in anesthetized dogs (Mitchell 1964; Brown et al. 2002a; Brown et al. 2002b).

### 6.2. The Nociceptive Withdrawal Reflex (NWR)

In humans a reflex withdrawal reaction can be elicited by transcutaneous electrical stimulation of a sensory peripheral nerve and the electromyographic response recorded from the flexor and extensor muscles. This nociceptive withdrawal reflex (NWR) is a polysynaptic spinal nociceptive reflex, and represents the mechanism for withdrawing an extremity from injury (Sherrington 1910). The NWR is reproducible, stimulus-dependent and is closely correlated with the intensity of subjective pain perception (Willer 1977; Willer 1984; Chan & Dallaire 1989). Therefore the NWR and its modulation have been widely used in experimental (Hagbarth 1960; Kugelberg et al. 1960; Hugon 1973; Willer & Bathien 1977; DeBroucker et al. 1989; Arendt-Nielsen et al. 2000; Andersen 2007) and pharmacologic studies (Willer & Bathien 1977; Willer 1985; Arendt-Nielsen et al. 1990; Petersen-Felix et al. 1995; Curatolo et al. 1997; Petersen-Felix et al. 1998; Piguet et al. 1998; Escher et al. 2007) as a noninvasive neurophysiologic tool to objectively assess spinal nociceptive processing. By applying appropriate repetitive stimulation patterns, temporal summation can be evoked and quantified by a facilitation of the reflex (Andersen et al. 1994; Arendt-Nielsen et al. 2000; Serrao et al. 2004). Temporal summation in humans has been considered as a psychophysical correlate of the early phase of wind-up. This facilitation of the nociceptive reflex response has been used as a tool to study and quantify aspects of central integration and sensitisation in humans (Kugelberg et al. 1960; Shahani & Young 1971; Hugon 1973; Akopian et al. 1996).

Electromyographic recordings of flexion reflexes of the limbs elicited by electrical stimuli have been investigated in decerebrated or spinalized rats (Schouenborg & Dickenson 1985; Schouenborg & Kalliomaki 1990; Schouenborg et al. 1995; You et al. 2003b; You et al. 2004), cats (Sherrington 1910; Schomburg 1990a; Levinsson et al. 1999), and rabbits (Clarke & Harris 2001). Unfortunately these models are of limited clinical interest because of their invasiveness and the influence of anesthetics on the flexion reflexes. Aware of this drawback, Carstens and coauthors measured the limb flexion withdrawal elicited by noxious thermal stimulation of the hindpaw in conscious rats (Carstens & Ansley 1993). Recently, results of a series of studies demonstrated the feasibility of evoking and recording the NWR for the fore- and hind limbs in standing, conscious horses (Spadavecchia et al. 2002; Spadavecchia et al. 2003; Spadavecchia et al. 2004; Spadavecchia et al. 2005), suggesting that the NWR could be used as a non invasive, objective method to measure nociception in this species.

# 7. Aim of the PhD project

With a cross-species approach based on the capability to investigate objectively and non-invasively the nociception-related responses in humans and in standing horses, it was assumed that a similar investigation in conscious, non medicated dogs would be possible.

The aims of the PhD project presented here were:

- To demonstrate the feasibility of evoking the NWR from the forelimb and hind limb in conscious, non medicated dogs, and score the behavioral responses to the electrical stimuli.
- 2) To study the modulation of the reflex after repeated electrical stimulations (temporal summation)
- 3) To investigate the pharmacological modulation of the NWR and temporal summation in dogs.

To develop a new, non invasive model of nociception in dogs would allow to gain species-specific knowledge about the nociceptive process and to obtain comparative physiologic data for a better understanding of nociception in general. The pharmacological modulation of the reflex would provide objective evidence on the efficacy of analgesic drugs in dogs.

The experimental work has been published in four papers dealing with the technical and physiological aspects of the canine NWR and its pharmacological modulation (Figure 1). This thesis presents and discusses the experimental work and the results obtained.

In the <u>first paper (I)</u> the feasibility of evoking the NWR by electrical stimulation of a sensory nerve and recording of the electromyographic response in both the forelimb and the hind limb, in conscious non medicated dogs is described. The recruitment of the NWR obtained with graded suprathreshold stimulations as the correlation between reflex characteristics and evoked behavioral responses were studied. The effect of the stimulus paradigm was analysed.

The <u>second paper (II)</u> investigated the facilitation of the NWR by repeated electrical stimuli and the associated behavioral response scores in conscious, non-medicated dogs as a measure of temporal summation. The influence of different stimulus intensities and frequencies on temporal summation was evaluated.

In the <u>third paper (III)</u> the effects of a tranquillizing dose of acepromazine on the NWR and temporal summation were analyzed. As a second objective the repeatability and stability of the NWR thresholds were investigated.

In the <u>fourth paper (IV)</u> the NWR and its facilitation evoked by repeated stimulations were used for the first time as a model to objectively and quantitatively analyze the antinociceptive properties of a usual low-dose constant rate infusion of ketamine in conscious dogs. Low-dose ketamine CRI has gained popularity in the management of post-operative pain in canine patients.

The conclusions outline the main findings and their clinical relevance and possible future implementations.

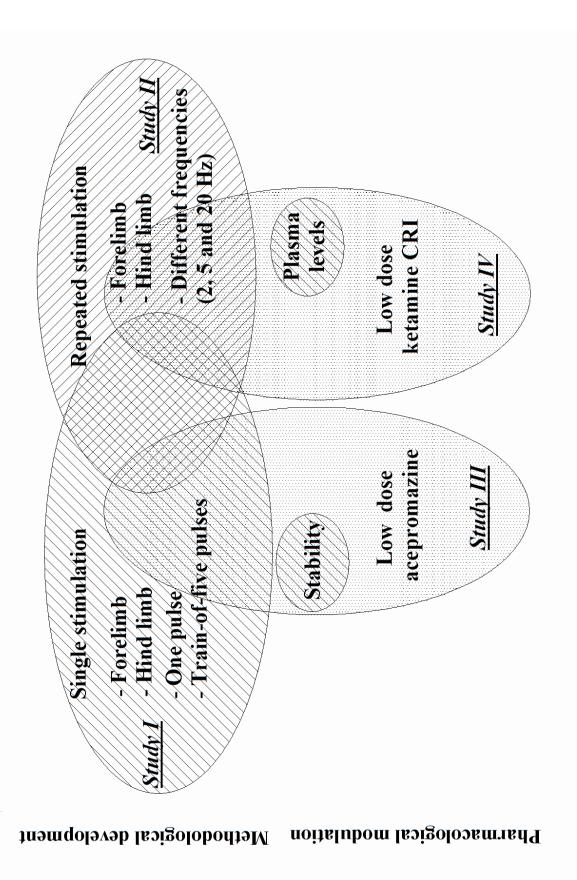


Figure 1. Schematic representation of the content of the PhD thesis

# 8. Methods

In this chapter the methods used to evoke record and quantify the NWR and the reflex facilitation after repeated stimulations in dogs will be described and discussed.

The experiments were approved by the committee for animal experimentation of the canton Basel city, Switzerland (approval number 2090).

# 8.1. The experimental dogs

For developing a new model of nociception care was taken to have a homogeneous group of dogs of the same breed and gender for the similarity in size, anatomy, metabolic and genetic characteristics. Thanks to a collaboration with Novartis Pharma based on the 3Rs concept "*replace, reduce, refine*" (Russell 1995) we enrolled eight adult male purpose-bred Beagles. The group consisted of young animals in training. The possibility to utilize these dogs avoided unnecessary recruitment of experimental animals and reduced costs. Dogs were housed together in runs (10 dogs/run) and were fed a maintenance formula once a day.

During preliminary work, the dogs were trained to lay in lateral recumbency. Only subjects with calm character and accepting to remain in lateral recumbency without restrain were selected. The dogs underwent clinical examination, and haematological and biochemical analyses were performed to assess health state.

Food was withheld in the morning of the experimental session. Only one dog at time was present in the laboratory. The laboratory room was kept at constant temperature (22°C) by the ventilation system and external noise was dampened. The dogs were controlled for one week after the experiments and than once 6 months later for possible skin changes at the site of electrodes application. No adverse effect was noticed except a slight local erythema for 3 days after shaving.

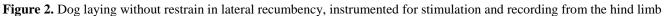
# 8.2. Eliciting and recording NWR in dogs

In experimental human studies, the NWR was elicited by heat via a laser beam (Willer et al. 1979; Mørch et al. 2007) or electrical stimulations (Willer 1983; Desmeules et al. 2003). Electrical stimulation may be of a pure sensory nerve (Arendt-Nielsen et al. 1995; Banic et al. 2004) or cutaneous, i.e. the foot sole (Andersen et al. 1999). In animal studies the NWR was elicited by thermal (Schouenborg & Dickenson 1985; Le Bars et al. 2001) and electrical (Spadavecchia et al. 2002; Spadavecchia et al. 2004) stimulations. Electrical stimulation was chosen as nociceptive stimulus in the present experiments (I to IV) for its capacity to elicit stable and reproducible reflexes. The electrical stimulus bypasses the peripheral receptors and depolarize the nerves directly, eliminating the delay in the latency of the reflex due to the peripheral transduction mechanism. Furthermore by choosing the intensity of the stimulus it is possible to target the desired fibres. Typically, with lower current intensities the larger fibres are activated while higher intensities are needed to depolarize also the thinner fibres (Wall & Woolf 1984).

# 8.2.1. Positioning of the dogs

The dogs were placed in right lateral recumbency (I-IV), as it is a physiological, species-specific sleeping position, in a comfortable, corncob-balls filled dog bed that took the shape of the body. The limbs were extended laterally in a natural position but not supported, without weight bearing or movement restriction of the nondependent limb. This position can be compared to the sitting position in humans (Willer 1977; Willer 1983; Rossi & Decchi 1994; Andersen et al. 1995b), where the volunteers have the limbs positioned so as to achieve complete muscle relaxation (Figure 2).





# 8.2.2. Stimulating and recording material

Stimulation and recordings were performed by use of a specially designed, computerized system (I-IV). The final stage of the electrical stimulator that received input from the computer was a battery-powered optoisolated constant-current device with a maximum voltage of 100 V and a maximal current of 40 mA. Electromyographic signals were amplified with an overall gain of 5,000 and bandpass of 7 to 200 Hz (first-order active filters with 6 dB/octave slope). They were passed through a digital converter to a computer for further processing and storage.

Electrical current was delivered via self adhesive electrodes (Spadavecchia et al. 2002; Spadavecchia et al. 2004; Andersen 2007). The stimulation electrodes (Neuroline 700 05-j, Medikotest A/S, Olstykke, Denmark) were placed over purely sensory nerves: the dorsal branch of the ulnar nerve at the level of the left fifth metacarpal bone of the forelimb (Figure 3A) and over the lateral plantar digital nerve of the hind limb at the level of the fourth metatarsal bone, just distal to the base and proximal to the head of each bone (Figure 3B).





Figure 3A and B. Detail of the stimulation sites

The electrodes were placed parallel to the nerve with the anode in the distal position, with an interelectrode distance of 0.8 cm. The distal portion of the limb was bandaged to prevent dislocation of the electrodes. The ground electrode (Synapse 32 mm, Ambu A/S, Ballerup, Denmark) was placed over the plantar side of the right foot and taped in place (Figure 1). Flexible leads were connected to the electrodes. The resistance of each electrode pair was checked and confirmed to be less than 5 k $\Omega$  before starting and at the end of each experimental session. Typically the resistance was between 1 and 3 k $\Omega$ . This is necessary to ensure that the nerve stimulator can deliver enough current to elicit the reflex in a stable and reproducible manner. To achieve low resistance, the skin was carefully clipped, shaved and degreased before electrodes application.

The same electrode type was used to record the surface electromyograms from the forelimb and hind limb muscles. Special care was taken to place the electrodes over the muscle bellies at a distance of 1 cm to avoid multichannel cross-talk contamination from adjacent muscles and minimize common-mode noise (Farina et al. 2002). Their position was marked with a pen, which allowed for exact repositioning in case the electrodes were disconnected.

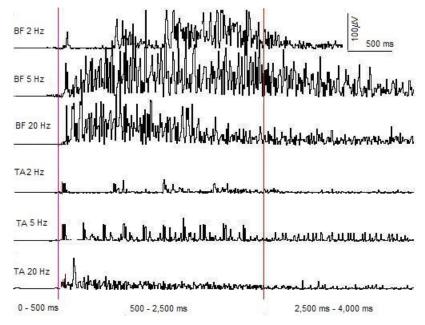
#### 8.2.3. Stimulus parameters

<u>Single stimulation.</u> In the published literature (Spadavecchia et al. 2002; Andersen 2007) a train-of-five pulses delivered at high frequency, which humans perceive as a single stimulus, is described as a standard stimulus to elicit the NWR. Along with other factors, the number of pulses and stimulus duration can influence the NWR (Tørring et al. 1981). The effect of stimulus configuration on the canine NWR was evaluated by using a single 1 ms pulse stimulus compared to a train-of-five 1 ms pulses delivered at 200 Hz (total duration 25 ms) (I). The stimulus configuration did not influence the latency of the canine NWR but the single 1 ms pulse stimulus resulted in a less reproducible reflex and of significantly lower amplitude. The train-of-five pulses was used as a standard stimulus paradigm in dogs (I-IV).

<u>Repeated stimulations</u>. Several stimuli configurations have been used in experimental studies in humans combining different numbers of pulses with a fixed frequency or different frequencies (ranging from 0.5 to 20 Hz) with a fixed number of pulses. Stimulus configuration is reported to affect the characteristics of

the reflex response (Arendt-Nielsen et al. 1994; Arendt-Nielsen et al. 2000; Bajaj et al. 2005). The effect of three stimulation frequencies on the characteristics of the canine reflex was investigated in study II: 2 Hz with 4 pulse trains, 5 Hz with 10 pulse trains and 20 Hz with 40 pulse trains (II) while the total duration of the stimulus (2 s) was kept constant (Arendt-Nielsen et al. 2000; Spadavecchia et al. 2004) (Figure 4). The frequencies used are in the range of spontaneous firing of damaged A $\delta$  fibres (0.1–30 Hz) (Devor 1994). Other study designs would have been possible: *i*) varying number of stimuli with fixed frequency, *ii*) different frequencies with fixed number of pulses or *iii*) different frequencies and different number of stimuli mixed in a way so that the duration of the train is constant. In study II option *iii*) was selected with a fixed duration of 2 seconds, in accordance with previous studies (Arendt-Nielsen et al. 2000) as time is essential when integration over time is to be studied. Like in horses (Spadavecchia et al. 2004), the stimulus frequencies used did not influence the canine temporal summation thresholds TS<sub>t</sub>.

Still at 20 Hz, reflex facilitation effectively dissipated with a significant reduction in the root-mean-square amplitude of the reflex activity during the final part of the stimulus series, compared with the other frequencies. This can be explained by habituation or activation of descending inhibitory systems in agreement with studies in men (Bajaj et al. 2005) and rats (You et al. 2003a; You et al. 2004). The highest correlations between stimulus intensity, relative reflex amplitude, and behavioral reaction scores were obtained at the 5 Hz frequency, which therefore is recommended as the standard for future studies in dogs.



**Figure 4.** Electromyograms obtained form the biceps femoris (BF) and tibialis anterior (TA) muscles with a repeated stimulus at 0.7 x  $I_t$  intensity for the 2, 5 and 20 Hz stimulus frequencies from one dog. The 500 to 2500 ms stimulation epoch is indicated by the vertical lines (abscissa: time in milliseconds; ordinate: amplitude of the reflex in  $\mu$ V).

# 8.3. Behavioural reactions

In humans, the value of the reflex amplitude is related to that of subjective pain intensity; therefore, the NWR model is an interesting tool for correlation of an electrophysiologic measure with pain in experimental studies (Willer 1983; Sandrini et al. 1993). To quantify the subjective pain sensation, a visual analogue scale is generally used. Use of such a scale is obviously not possible in animals and behavioral responses were used as a psychophysical correlate of the dogs' perception of the electrical nociceptive stimuli. A 6-point behavioral scoring system was developed and applied as an analogue of the visual analogue scale (Table 1; I to IV). Each numerical score corresponded to a precise behavioral pattern. The scoring system was adequate to describe the pattern of reactions and to detect changes related to differences in stimulus intensity (I). With suprathreshold intensities typically the dogs looked at the stimulated leg or stiffened or attempted to stand, revealing general awareness. This might indicate that the evoked responses and thus the recorded reflex EMG activity, contain also a supraspinal (possibly cortical) component.

For studies II to IV a new scoring system was developed as the behavioral responses were more complex when repeated stimulations were used. The behavioral patterns were quite stereotyped and differed from the behavioral reactions observed when a single stimulus was applied (I); for example, localized muscle twitches with a repeated stimulus at sub-threshold intensity were never detected after application of a single stimulus. At temporal summation threshold intensity i.e., the entire limb was flexed and flexion maintained whereas only a weak localized joint flexion was induced with a single stimulus at the same intensity. This can be interpreted as the nociceptive impulse being perceived more intensely and prolonged in accordance with human reports (Price et al. 1978; Arendt-Nielsen et al. 1994; Andersen et al. 1995a; Arendt-Nielsen et al. 2000).

#### 8.4. Analysing the NWR

To quantify the electromyographic response two parameters were used: response delay as latency, and magnitude as RMS amplitude (I-IV).

8.4.1. Onset latency

The onset latency of the NWR was defined as the time elapsed from the stimulus onset to the reflex onset (EMG deflection). In the present work this was determined by visual inspection of the records using a measurement cursor.

# 8.4.2. Reflex magnitude

In the literature different methods, such as peak amplitude of the rectified EMG (Willer et al. 1978), peak to peak measures (Knobloch et al. 2006), root-mean-square (RMS) (Andersen 2007) and area-under-the rectified curves (Chan & Dallaire 1989), have been used to quantify the EMG activity .

<u>Single stimulation.</u> The RMS amplitude of the reflex was calculated in fixed post-stimulation epochs (I-IV). Considering that there was a variable degree of EMG activity at rest, the ratio of the RMS amplitude of the reflex for each epoch to the RMS background EMG amplitude was calculated in order to minimize the influence of variability among dogs (I to IV).

<u>Repeated stimulations.</u> To quantify the magnitude of the reflex response and reduce interindividual variability, the relative amplitude was calculated as the ratio between the mean RMS reflex activity of each 20 to 100 millisecond (50 milliseconds for 20 Hz) post stimulation interval in the stimulation epoch and the RMS background activity (II). Thereafter (III-IV) the area-under-the relative reflex amplitude in the 20 to 100 ms epoch following each repeated stimulus (temporal summation curve) was calculated.

#### 8.4.3. Single NWR and temporal summation thresholds

In the present studies (I-IV) the individual NWR threshold intensity  $I_t$  was defined as the minimum stimulus intensity that evoked EMG activity from the deltoideus muscle (forelimb) and the biceps femoris muscle (hind limb) in the 20 to 100 millisecond epoch with an amplitude >10 times the EMG background activity, and a duration > 10 milliseconds. To reduce intra- and interindividual variability it was associated with an evoked behavioral reaction score between 1 or 2 (Table 1). The detected threshold intensity was repeated 3 times to confirm the reproducibility of the response; if not reproducible, the current intensity was increased by 0.2 mA and the threshold assessment repeated.

The temporal summation threshold (TS<sub>t</sub>) definition used for dogs was based on review of the human literature, in which various definitions have been proposed (Andersen et al. 1994; Andersen et al. 1995a; Petersen-Felix et al. 1995; Petersen-Felix et al. 1996; Arendt-Nielsen et al. 2000; Serrao et al. 2004; Andersen 2007). Among those reports, the increase in amplitude of the last 1 or 2 reflexes above a certain limit was considered indicative of facilitation. The canine temporal summation threshold TS<sub>t</sub> (II to IV) was defined as the intensity at which the RMS amplitude of the EMG signal in the 20 to 100 millisecond interval increased and exceeded 10 times the background activity from the third or fourth stimulus of the pulse train and was associated with a clear behavioral reaction scored as  $\geq 2$ . To assess the temporal summation by the size of one reflex response only would have been too sensitive to the natural variation in reflex amplitude and possible technical artifacts. The 3<sup>d</sup> and 4<sup>th</sup> train were selected to be able to compare consistently the three frequencies studied considering the lower number of stimuli (4) for the 2 Hz.

# 9. Physiology of the canine NWR

### 9.1. Functional significance

The "flexion reflex" is the mechanism for withdrawing a limb from a noxious stimulus (Sherrington 1910; Shahani & Young 1971; Schomburg 1990b) consisting of activation of flexor and inhibition of

extensors muscles from large receptive fields. Recently this "flexion reflex" concept has been refined by the "modular organization" concept. Studies in rats (Schouenborg & Kalliomaki 1990), cats (Levinsson et al. 1999) and humans (Andersen et al. 2001; Andersen 2007) showed that each muscle or group of synergistic muscles involved in the withdrawal of the limb is activated by stimulating a specific skin area, its " receptive field". The cutaneous receptive field corresponds closely to the skin area withdrawn upon contraction of the associated muscle. This modular concept indicate that the nociceptive withdrawal movement is not a trivial generalized flexion of the limb but a selective activation of the relevant muscles, making the simple "sherringtonian flexion reflex" a sophisticated, highly functional and adaptable reflex system.

For a thorough description of the NWR in dogs, the EMG activities of 2 flexor muscles for each limb were studied (I, II): the deltoideus and cleidobrachialis muscles for the forelimb and the biceps femoris caput pelvis and the tibialis anterior muscles for the hind limb (Figure 5 A and B). Those muscles are relatively superficial and easy to localize. These anatomic characteristics allowed for standardized positioning of the EMG electrodes, with minimal multichannel cross-talk contamination from adjacent muscles, and common mode noise (Farina et al. 2002).

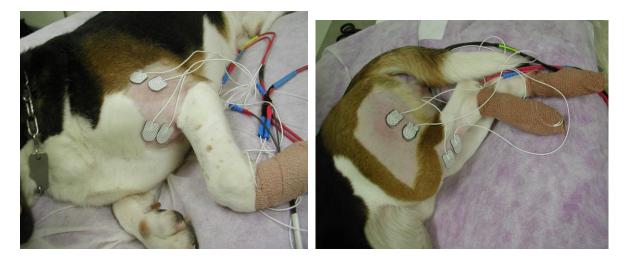


Figure 5 A). Recording electrodes over the deltoideus and cleidobrachialis muscles of the forelimb. B) Recording electrodes over the biceps femoris and tibialis anterior muscles of the hind limb.

#### 9.2. Forelimb muscles

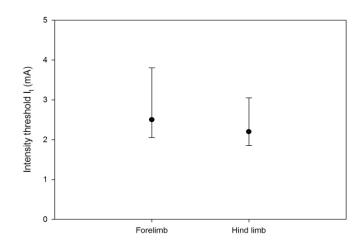
It was assumed that the withdrawal response of the limb evoked by electrical stimulation could be compared with the withdrawal movement to overcome an obstacle during deambulation. The initial movement is a flexion of the shoulder joint together with a locking of the elbow joint and dorsiflexion of the carpus, which activates the deltoideus and cleidobrachialis muscles. The principal functions are flexion and protraction of the shoulder joint and flexion of the elbow joint, respectively These muscles offer the largest and longest duration reflex responses in kinematic and EMG analysis of cutaneous reflexes in cats (Drew & Rossignol 1987). Furthermore, results of a previous study (Kolb et al. 1997) in cats have indicated that the cleidobrachialis muscle has a burst of EMG activity that coincides with the evoked forelimb withdrawal response.

#### 9.3. Hind limb muscles

The tibialis anterior muscle dorsiflexes and supinates the ankle joint. Correspondingly, its receptive fields covers the distal and medial site of the paw in rats (Schouenborg & Kalliomaki 1990). The caput pelvis of the biceps femoris muscle flexes the stifle joint and acts to withdraw the foot irrespectively of whether the foot is in contact with the ground (Levinsson et al. 1999). Its receptive field is relatively large and covers the entire paw and part of the anterior side of the lower hind limb in rats (Schouenborg & Kalliomaki 1990; Carstens & Ansley 1993). In humans, the biceps femoris muscle has the earliest reflex activity (Hugon 1969) and the tibial muscle has been found to be most representative in the measurement of responses of the NWR (Pedersen 1954; Shahani & Young 1971). Therefore, it seemed appropriate to record the NWRs of the hind limb in dogs from these flexor muscles (Figure 5 B).

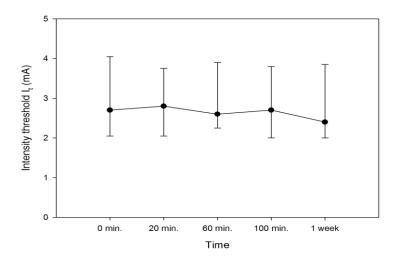
#### 9.4. The NWR threshold intensity (I<sub>t</sub>) in dogs

Compared to horses (Spadavecchia et al. 2003) dogs did not show a significant difference in threshold stimulation intensities between front and hind limb (I). The median  $I_t$  are shown in Figure 6.



**Figure 6**. Median (25-75% IQR) NWR thresholds  $I_t$  for the forelimb and the hind limb of the 8 dogs. No significant difference was found between limbs (Wilcoxon test).

In study III we analyzed the short-term (within session) and the long term (1 week) variability of the NWR thresholds ( $I_t$ ) and temporal summation ( $TS_t$ ) thresholds (Figure 7). We could show that the NWR thresholds are stable over time and the model is reproducible and robust. The evidence of the measurement reliability in dogs is very important if within-subject variations in  $I_t$  are to be attributed to modifications in central excitability or to efficacy of antinociceptive drugs (French et al. 2005).



**Figure 7.** Median (25-75% IQR) forelimb reflex thresholds  $I_t$  of 8 dogs. No significant short term and long term variability were found (Friedman repeated measures ANOVA).

### 9.5. Reflex components

To separate reflex components of various origins, the 400 milliseconds post stimulation interval corresponding to the EMG recording time was divided into 3 epochs: 0 to 20 milliseconds, 20 to 100 milliseconds, and 100 to 400 milliseconds. These epochs were defined on the basis of the conduction velocities of the canine nerve fibers (Gasser & Erlanger 1927; Burgess & Perl 1967) and the conduction pathway lengths of the Beagles (Figure 8).

9.5.1. The early reflex activity: 0 to 20 milliseconds epoch

The first epoch is preferentially reflecting non-nociceptive components resulting from the activation of A $\beta$  afferent nerve fibers. The short latency reflex component of tactile origin has been described for the upper (Cambier et al. 1974) and lower limb (Hugon 1969; Willer 1977) in humans and in horses in the (Spadavecchia et al. 2002; Spadavecchia et al. 2003). Its occurrence is highly variable. Based on the conduction velocity of the sensory afferent fibers in dogs (ulnar nerve:  $69.4 \pm 6.9$  m/s; tibial nerve:  $63.4 \pm 5.3$ m/s) (Redding et al. 1982), for a mean afferent distance of 38.5 cm, after adding a mean efferent time of 2.5 milliseconds and an overall time of 5 milliseconds for spinal and motor endplate delay, the latency of the canine early reflex should be approximately 14 milliseconds.

At  $I_t$ , none of the dogs showed a clear early reflex between 0 and 20 ms neither for the forelimb nor for the hind limb muscles.

### 9.5.2. The NWR: 20 to 100 milliseconds epoch

In the experimental beagles (I to IV), taking into account the A $\delta$  fiber conduction velocity range (4 to 30 m/s) for the afferent component (Gasser & Erlanger 1927; Heinbecker et al. 1933; Burgess & Perl 1967) and a mean afferent distance of 38.5 cm, after adding a mean efferent time of 2.5 milliseconds and an

overall time of 5 milliseconds for spinal and motor endplate delay, the NWR should occur in the 20 to 100 milliseconds post-stimulation epoch. These calculated latencies matched our experimental findings, confirming the nociceptive origin of the reflex.

# 9.5.3. The late reflex activity: 100 to 400 milliseconds epoch. Preliminary work

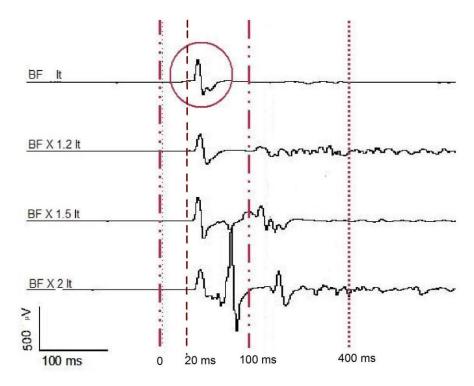
The 100 to 400 milliseconds epoch most likely contains reflex components of mixed spinal and supraspinal origin (Le-Bars et al. 1992; Andersen et al. 1999). In men, the late reflex activity have be recorded episodically from the biceps femoris, rectus femoris and more consistently from the tibialis anterior muscles (Shahani & Young 1971; Roby-Brami & Bussel 1987). In dogs, the late reflex activity could be recorded from the deltoideus and cleidobrachialis muscles in 0/8 and 0/8 dogs respectively with the one pulse stimulus paradigm, and in 3/8 and 0/8 dogs with the train-of-five pulses stimulus paradigm. Late reflex activity was recorded from biceps femoris and tibialis anterior muscles respectively in 2/8 and 3/8 dogs with the one pulse stimulus paradigm, 6/8 and 8/8 dogs with with the train-of-five pulses stimulus paradigm (I). This late reflex activity occurred 87.1 to 200 ms post-stimulation, being most pronounced with the train-of-five pulses and almost not present for the single pulse paradigm unless suprathreshold intensities were used. A tendency to increased reflex size with suprathreshold stimuli was observed (Figure 8; Table 2).

On the basis of canine C fibres conduction velocity range (0.8 to 1.5 m/s) (Iriuchijima & Zotterman 1961) for the afferent component, after adding a mean efferent time of 2.5 milliseconds and an overall time of 5 milliseconds for spinal and motor endplate delay, the late EMG response in dogs should occur between 241 and 818 ms. This agrees with C fibres activity recorded in spinal cats (Le Bars et al. 1976). Thus, it seems unlikely that the late EMG activity recorded in I is related to C fibres activation. Additionally the stimuli intensities used here (up to 2 X I<sub>t</sub>) are below intensities needed to activate C fibres (Le Bars et al. 1976) since it is known that C fibres threshold is 4 –5 times higher than that of A $\delta$  fibres. Hence, it would be necessary to stimulate the dogs with intensities of 4 to 5 X I<sub>t</sub> to activate C fibres.

According to recent work the limits for conduction velocities of A $\delta$  fibres are not so clearly demarcated, with some A $\delta$  fibres having conduction velocities as low as 2.5 m/s associated with higher thresholds (Kumazawa & Mizumura 1987; Djouhri & Lawson 2004). By taking into account this conduction velocity, the reflex activity would occur 100 to 192.5 milliseconds after stimulation. The calculated latency fits with the recorded late reflex activity assuming a direct spinal loop.

Furthermore it is important to remind that in this time frame it is not possible to exclude a supraspinal loop but more invasive investigations are needed to confirm this hypothesis.

The significant higher incidence in the hind limb compared to forelimb could suggest different functional adaptation of the limbs.



**Figure 8.** Records form the Biceps Femoris muscle. Stimulations at threshold  $(I_t)$  and suprathreshold  $(X I_t)$  intensities. The dotted lines delimitate the epochs.

9.5.4. Eliciting the NWR in dogs: conclusions

The analysis of the recruitment curves showed a positive correlation between the intensity of stimulation, the amplitude of the reflex and the behavioral reaction scores, confirming the nociceptive origin of the NWR. In dogs the NWR is a complex reflex, whose nociceptive component is only a part of the flexion reflex circuitry.

### 9.6. Facilitation of the NWR by repeated stimulations

#### 9.6.1. Wind up and temporal summation

In neurophysiologic experimental settings, repetition of a fixed supramaximal stimulus at low frequency activates afferent C fibres, which causes an augmented firing of the dorsal horn WDR neurons (Dubner 1991) followed by afterdischarge and increased sensitivity (Price 1972). This activity-dependent facilitation was termed wind up (Mendell & Wall 1965). The voltage and ligand gated NMDA-receptors are important for wind up in WDR-neurons. The ongoing afferent input from the C fibres depolarizes the WDR neurons thus opening the channel (unplugging the  $Mg^{2+}$  ion in the ion channel). The intracellular  $Ca^{2+}$  concentration further depolarise the cell which activates a protein kinase that contributes to keep the NMDA channel open, increasing the sensitivity to glutamate (Dickenson 1995; Woolf 1996).

Wind up is only the initial step of the long-lasting state of neuronal hyperexcitability and plastic changes that develop during central sensitization (You et al. 2004) which may lead to chronic pain states (Arendt-

Nielsen et al. 1994; Dickenson 1995; Guirimand et al. 2000). In between other causes, central sensitisation can be initiated by surgery (Wilder-Smith & Arendt Nielsen 2006).

Studies in rats (Dickenson & Sullivan 1987; Schouenborg & Dickenson 1988), cats (Price 1972), horses (Spadavecchia et al. 2004; Spadavecchia et al. 2005) and humans (Arendt-Nielsen et al. 1994; Arendt-Nielsen et al. 2000) have revealed that application of repeated electrical stimulations results in facilitation of the NWR, as a result of the temporal summation of action potentials at the level of the spinal dorsal horn neurons. Clinically it is accompanied by an amplified sensation of pain (Hugon 1973; Andersen et al. 1995a). Therefore in humans, the psychophysical and electrophysiologic responses to repetitive nociceptive stimulations have been assessed as a noninvasive experimental surrogate of windup (Herrero et al. 2000; Desmeules et al. 2003). The facilitation of the NWR by repeated stimulations has been used to investigate the degree of sensorial dysfunction (Curatolo et al. 1995; Desmeules et al. 2003; Banic et al. 2004) and evaluate the analgesic efficacy of drugs in experimental and clinical setting in humans (Willer & Bathien 1977; Price et al. 2004; Spadavecchia et al. 2000; Bossard et al. 2002; Escher et al. 2007) and animals (You et al. 2003a; You et al. 2004; Spadavecchia et al. 2005; Knobloch et al. 2006; Spadavecchia et al. 2007).

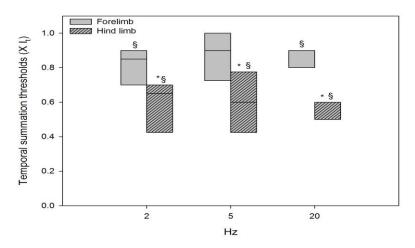
Summation of afferent activity seems to be more pronounced for C fibres mediating second pain compared to A $\delta$  fibres mediating first pain (Price 1972; Sivilotti et al. 1993).

Many human studies (Andersen et al. 1994; Arendt-Nielsen et al. 1994; Arendt-Nielsen et al. 2000; Serrao et al. 2004) on temporal summation concentrated on the facilitation of the NWR reflex mediated by A $\delta$  fibres. Activation of A $\delta$  fibres causes a central discharge that lasts several hundred milliseconds (Foreman et al. 1975) which can explain why repeated nociceptive electrical stimuli result in facilitated polysynaptic reflexes.

# 9.6.2. Temporal summation in conscious dogs (II-IV)

In the studies II to IV, the analysis of the reflex activity focused on the A $\delta$  fibres evoked activity expressed in the 20 to 100 ms post stimulus intervals. On the basis of canine C fibres conduction velocity range (0.8 to 1.5 m/s) (Iriuchijima & Zotterman 1961), the reflex activity due to C fibres activation would appear later, between 250 and 830 ms after each stimulus (Gasser & Erlanger 1927; Hallin & Torebjork 1973; Hugon 1973). Therefore it might be possible, at least with suprathreshold intensities, that C fibres activity evoked by the first stimuli summates with A $\delta$  activity evoked by the last stimuli in the 2 s epoch. In dogs (II) the facilitation of the NWR for the forelimb and hind limb occurred at intensities that were significantly lower than I<sub>t</sub> (Figure 9). At temporal summation intensity TS<sub>t</sub>, the entire limb was flexed, whereas only localized joint flexion was induced with a single stimulus; indicating that the nociceptive impulse was perceived more intensely despite the lower intensity, in accordance with findings in humans (Price et al. 1978; Arendt-Nielsen et al. 1994; Andersen et al. 1995a; Arendt-Nielsen et al. 2000).

The intensities needed to facilitate the reflex where significantly higher for the forelimb, for all frequencies. The reason for this remains unclear. In humans, few investigations (Bromm & Treede 1980; Serrao et al. 2006) have analyzed the forearm NWR. In horses, the NWR and its facilitation have been studied for both fore- and hind limbs (Spadavecchia et al. 2003; Spadavecchia et al. 2004) and only minor differences in the characteristics of temporal summation between the limbs were noticeable with repeated stimulations. Whether the spinal neuronal organization of the fore- and hind limb differs or the supraspinal modulation for the forelimb is more pronounced than that for the hind limb in dogs will require verification in future studies. It might be assumed on a functional, biomechanical basis that the sustaining forelimb would be less sensitive to nociceptive stimuli compared to the propulsive hind limb.



**Figure 9.** Median (25-75% IQR) temporal summation thresholds (TS<sub>t</sub>) of the 8 dogs of the study (II) expressed as a fraction of the NWR threshold intensity I<sub>t</sub>. The I<sub>t</sub> fractions needed to facilitate the reflex were significantly lower than I<sub>t</sub>, except for the 5 Hz when corrected for multiple testing (§; Friedman ANOVA followed by a Tuckey test). \* Between limbs differences (p< 0.05 Wilcoxon signed rank test).

#### 9.6.3. Temporal summation in conscious dogs: conclusions

The intensity of stimulation affected the magnitude of the reflex response with a significant positive correlation between the stimulus intensity-response curve and the reflex amplitude-response curve; on the basis of neuronal recordings in other species, this is probably attributable to spatial summation of the afferent information at spinal level (Arendt-Nielsen et al. 2000; You et al. 2003b). The behavioral response scores increased with increasing stimulation intensities as an indication of increased nociception. This positive correlation between intensity, relative amplitude, and behavioral response scores confirmed the consistency of experimentally induced temporal summation in dogs. Temporal summation was more easily elicited from the hind limb compared to the forelimb, the reason for this difference remaining to be elucidated.

The temporal summation can be used as a model of wind-up in canines both for better understanding of pathophysiology of chronic pain states and to prove specifically and objectively in pharmacodynamic studies the efficacy of analgesic drugs in this species as in study IV.

# 10. Variations in the canine reflex

#### 10.1. Posture

Numerous studies in humans have evaluated the NWR in the supine (Hugon 1973; Willer 1977; DeBroucker et al. 1989) and standing (Hagbarth 1960; Rossi & Decchi 1994; Andersen et al. 2003) positions. In horses, the NWR recordings were performed in the standing animal with full weight bearing (Spadavecchia et al. 2002; Spadavecchia et al. 2003). The dogs (I to IV) were non-weight bearing. The position and therefore the load to which the limb is submitted can modulate the NWR (Paquet et al. 1996; Andersen et al. 2003) with a significant inverse correlation between the load to which the limb is subjected and the size of the reflex response (Rossi & Decchi 1994). Thus, care should be taken when comparing results from different studies.

#### 10.2. Age, sex, circadian variations

In the present studies (I to IV) describing the NWR in conscious dogs, attention was paid to standardize and control for possible cofactors that could have influenced the results. The NWR threshold and reflex characteristics are influenced by the extreme of age (Sandrini et al. 1989; Edwards et al. 2003), therefore adult dogs were retained for the study. Results of clinical studies in humans (Desmeules et al. 2003; Banic et al. 2004) have indicated that NWR thresholds are often lower in individuals with pain disorders, compared with healthy persons. None of the dogs in the present study had a painful condition (as assessed by physical examination). Gender differences in the NWR thresholds are reported in humans (Serrao et al. 2006) with lower thresholds in females. This could be reconducted to the differences between sexes in the perception and modulation of pain reported for humans (Berkley 1997) and animals (Aloisi et al. 1994; Cook & Nickerson 2005) or to the differences in motor units of the constituent muscle fibres, thus influencing the onset latency and the peak-to-peak amplitude of the reflex (van Selms et al. 2005). Therefore only male dogs were studied (I to IV). All the experiments were performed at the same time of the day to minimize interindividual circadian variations in NWR thresholds (Sandrini et al. 1986). After instrumentation, the dogs received 4 test stimuli at different intensities to make them familiar with the experimental method prior to formal threshold measurement. It was noticed during pilot work in dogs that the reflex thresholds increased and then stabilized over time; this can be explained by high levels of anxiety, which may increase central excitability as indexed by lowering of NWR thresholds (Willer 1980; Willer & Albe-Fessard 1980; Willer 1983).

### 10.3. Habituation

By repeating electrical stimulations one can assist to a gradual decrease in the NWR amplitude, a purely spinal phenomenon defined as "habituation". Habituation is intensity and frequency dependent, occurring more frequently at low intensities and at high stimulation frequencies (Shahani & Young 1971;

Dimitrijevic et al. 1972). In all studies (I to IV), at least 60 s between successive single stimuli were allowed in order to avoid habituation which could have reduced reflex amplitude (Shahani & Young 1971).

When repeated stimulation were given (II) a decrease in the reflex facilitation was noticeable at all intensities with the 20 Hz frequency and only at suprathreshold intensities for the 2 and 5 Hz frequencies. This could be related to habituation but also to supraspinal descending inhibitory processes (Gozariu et al. 1997).

# 11. Pharmacological modulation of the NWR and temporal summation

Pharmacological modulation of the NWR is considered to occur when a drug modifies the NWR threshold intensity and reflex characteristics. Analgesic activity is generally attributed when an increase in the  $I_t$  or a reduction in the reflex amplitude or magnitude of temporal summation occur after its administration.

### 11.1. Low-dose acepromazine (III).

One of the future goals is to implement the NWR and temporal summation model in clinical practice (see later), as tools to detect and quantify the degree of sensory dysfunction in dogs affected from chronic malignant or non malignant pathologies. Therefore to augment the compliance of canine patients to the measurement technique, well-being and reduce stress, the pre-emptive administration of a neuroleptic drug would be indicated. The ideal drug should be anxyolitic, safe, and deprived of antinociceptive action which could exert a modulatory effect on the test altering its validity.

Based on clinical experience and previous work (Dasgupta & Werner 1955; Krivoy 1957; Silvestrini & Maffii 1959) it was hypothesized that 0.01 mg kg<sup>-1</sup> IV acepromazine would provide sufficient tranquillisation for the purpose of the recordings while having minimal impact on the model and side effects.

## 11.1.1. Use of phenotiazine tranquillizers in human and veterinary medicine

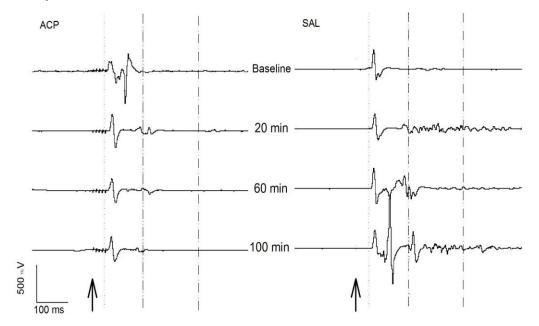
In human medicine, the phenotiazine derivatives, i.e. chlorpromazine, were very popular in the 1950s as major tranquillizers to treat psychosis and other major psychiatric disorders. They were also used as preanesthetic sedatives and for neuroleptoanalgesia (Brown 1969). Because of the major undesirable side effects as intraoperative hypotension and dysphoria, their use has been supplanted by the availability of the less toxic benzodiazepines. Neuroleptanalgesia remains a mainstay of veterinary anaesthesia and acepromazine, a member of the phenotiazine family, is the most widely used sedative (Barnhart et al. 2000b). Acepromazine effect is dose related. Doses below 0.03 mg kg<sup>-1</sup> it acts as a tranquillizer, exerting a calming effect on the behaviour of excitable animals with minimal cortical depression (Pugh 1964; Hall et al. 2001; Plumb 2002). With increasing dose sedation occurs, up to a plateau with prolonged duration

and higher incidence of side-effects. The central nervous system effects of acepromazine are attributed to its antagonistic action at the D1 and D2 dopamine receptors. The dopaminergic neurons are predominantly located in the reticular formation and modulate complex functions as arousal, movement, posture, pain, and autonomic function. They provide a major ascending input to the cerebral cortex and the basal ganglia, that is important for initiation of behavioural responses (Sapper 2000). Because of the depression of basal ganglia activity, care has to be taken in the interpretation of the antinociceptive activity of acepromazine when using models with behavioural endpoints (Steagall et al. 2008)

11.1.2. Effects of acepromazine on NWR and temporal summation in dogs

Low-dose acepromazine exerted a mild tranquillization lasting 30 minutes without modifying the NWR threshold nor the NWR characteristics recorded in the 20 to 100 ms interval as latency, amplitude and stimulus-response curve at any time point after administration (Figure 10). This indicates that acepromazine did not inhibit  $A\delta$  fibre evoked reflex activity nor affected the motor outflow. Our findings are consistent with previous work, where acepromazine did not alter the baseline nociceptive thresholds in a canine thermal and pressure nociceptive model (Barnhart et al. 2000b). Low-dose acepromazine did not affect the temporal summation threshold, nor the positive correlation between the magnitude of temporal summation (as measured by the area under the temporal summation curve) and its perception (as measured by the evoked behavioural response scores) confirming the consistency of this experimental model.

In conclusion, acepromazine can be used to facilitate data recording in anxious subjects without altering the validity of the NWR model.



**Figure 10.** Representative electromyograms evoked at  $I_t$  intensity recorded from the deltoid muscle of a dog before and 20, 60 and 100 min after drug administration. The arrow indicates the start of the electrical stimulus. The dotted to dash-dotted lines

represent the 20 to 100 ms epoch and the dash-dotted lines represent the 100 to 200 ms epoch. ACP: Acepromazine; SAL: saline.

#### 11.1.3. Phenotiazine analgesia: mythos or reality?

The analgesic activity of phenotiazines remains a controversial topic (McGee & Alexandre 1979). To date only for methotrimeprazine there is evidence for reliable dose related analgesia in men (McGee & Alexandre 1979; Patt et al. 1994). The exact mechanism of action is not clear (Roberts et al. 1982). Due to its depressing action on the reticular formation (Preston 1956; Engberg et al. 1968), acepromazine could modulate nociception by reducing the afferent information to the cortex or by enhancing the tonic activity of the descending inhibitory pathways. As stated in paragraph 9.5.3, the late reflex activity recorded in the 100 to 200 ms epoch should contain signals of mixed spinal and supraspinal origin. Therefore to specifically analyse this interval could improve the understanding of the mechanism of action of phenotiazine. Acepromazine at the dose used in study IV, didn't alter the late reflex activity when single or repeated stimulations were used, indicating that the supraspinal control of the reflex was comparable between treatments.

Our results confirm that low-dose acepromazine is deprived of antinociceptive properties in dogs (Gross 2001; Plumb 2002).

### 11.2. Low-dose ketamine constant-rate-infusion (IV)

Ketamine is a phencyclidine congener, and the molecule exists as two optical isomers R (-) and S (+) ketamine; the racemic mixture is currently used clinically. In veterinary medicine ketamine is commonly used for induction and maintenance of anaesthesia in a wide variety of species (Wright 1982). In men, it has found a niche for anaesthesia in emergency situations. Its usefulness however is limited by its undesirable psychic emergence effects.

The neuropharmacology ketamine is complex: the drug interacts with multiple binding sites, including Nmethyl-D-aspartate (NMDA) and non-NMDA glutamate receptors, nicotinic and muscarinic cholinergic, opioid and monoaminergic receptors. All of these interactions play a role in pharmacological and clinical properties of ketamine. However, the NMDA receptor antagonism accounts for most of the analgesic, amnesic, psychomimetic effects of the compound. From animal (Hao et al. 1998) and human (Woolf & Thompson 1991; Kohrs & Durieux 1998) experimental research there is evidence that due to its antagonistic action at NMDA receptors, ketamine can modulate spinal "wind-up" and central sensitisation in contrast to volatile agents such as isoflurane (Petersen-Felix et al. 1996). With a mechanism-based approach, ketamine has been used in humans to implement peri-operative pain management (Woolf & Max 2001; McCartney et al. 2004) and treat traumatic, neuropathic and chronic pain (Stubhaug & Breivik 1997; Carr et al. 2004). The clinical effects of ketamine are dose-dependent ranging from sedation with plasma levels close to 300 ng ml<sup>-1</sup> (Schmid et al. 1999; Rogers et al. 2004) to anesthesia when the plasma concentration is above 1,000 ng ml<sup>-1</sup> in humans (Domino et al. 1982) and above 3,000 ng ml<sup>-1</sup> in dogs (Kaka & Hayton 1980). In humans, to avoid the psychomimetic side effects which limit its clinical acceptance, low sub-anaesthetic doses (Schmid et al. 1999; Richebe et al. 2005) or the use of S-ketamine which produces fewer psychomimetic disturbances and less agitation than the racemic mixture (Hempelmann & Kuhn 1997) has been recommended.

# 11.2.1. Ketamine as an analgesic in dogs

Extrapolating from these encouraging results in man, low-dose ketamine is increasingly used in canines for its analgesic properties as part of a balanced anaesthesia /analgesia protocols. Slingby et al. (2000) described improved post-operative analgesia in dogs undergoing ovariohysterectomy after a 2.5 mg kg<sup>-1</sup> ketamine bolus. Still its antinociceptive effect was short lived and associated with excessive sedation. Therefore they suggested to administer ketamine by CRI to prolong the duration of analgesia and decrease the side effects as it is done in man (Schmid et al. 1999; Richebe et al. 2005). Wagner et al. (2000) added a low-dose ketamine CRI to the balanced anesthetic protocol in dogs undergoing forelimb amputation. They could show only slight improvement of the pain scores at 12 and 18 h post-operatively and activity scores 72 h post-operatively compared to saline. To date the published evidence of ketamine analgesia in dogs is scarce and no data is available on its effective antinociceptive plasma concentration in this species.

Therefore the aim of study IV was to evaluate quantitatively the antinocieptive efficacy of a usual lowdose ketamine CRI in dogs and to correlate its efficacy with the enantioselectively measured plasma levels of the drug and its metabolite norketamine.

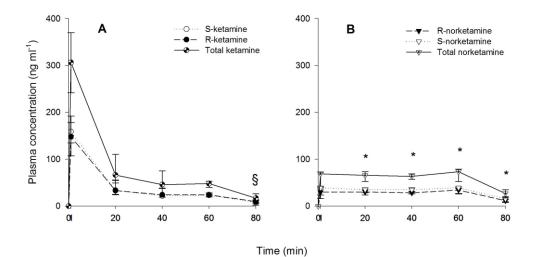
After baseline measurements a 0.5 mg kg<sup>-1</sup> loading bolus followed by 10  $\mu$ g kg<sup>-1</sup> min<sup>-1</sup> CRI of ketamine for 59 min were given intravenously (Figure 11). Electrophysiological measurements were repeated 1, 4, 8, 12, 20, 40 and 80 min post bolus. Contemporaneously, evoked behavioral responses and sedation were scored and side effects recorded by the mean of a purposefully developed sedation score (Table 3).



**Figure 11.** Beagle receiving the ketamine CRI delivered by a syringe pump in the right cephalic vein. Blood is sampled through a 3 way port from the left cephalic vein. The self-adhesive electrodes for recording of the surface EMGs from the biceps femoris, and tibialis anterior muscles and for transcutaneous electrical stimulation of digital plantar nerve are in place.

#### 11.2.2. Plasma concentrations of ketamine in dogs

Plasma concentrations of ketamine and norketamine were enantioselectively measured before, 1, 20, 40, 60 and 80 min post bolus (Figure 12 A and B). Unexpectedly the low-dose racemic ketamine CRI in conscious beagles resulted in low plasma levels (IV), which were in a 5 fold lower range compared to men receiving the same CRI regimen (Domino et al. 1982; Arendt-Nielsen et al. 1995). The reasons for the difference in ketamine plasma concentration between man and dog, the discordance with expected plasma levels with the available kinetic data in dogs (Kaka & Hayton 1980) will be addressed in detail in a future study using a physiologically based pharmacokinetic model (Knobloch et al. 2006).



**Figure 12. A)** Median (25% to 75% IQR) plasma concentrations of total, R- and S- ketamine (§ difference between enantiomers: P< 0.05; Wilcoxon test) and **B**) Median (25% to 75% IQR) plasma concentrations of total, R- and S- norketamine (\* difference between enantiomers; p< 0.05; Wilcoxon test) in 8 beagles during and after the ketamine CRI.

#### 11.2.3. Effects of ketamine on NWR and temporal summation in dogs

There was no effect of the low-dose ketamine CRI on the reflex threshold ( $I_t$ ) nor on the amplitude of the reflex elicited by a single stimulus. There was up to 81% reduction of the magnitude of temporal summation compared to baseline as an index of the antinociceptive effect of ketamine in dogs most likely via the NMDA receptor system (Figure 13). Also the behavioral reactions scored lower compared to baseline, confirming the antinociceptive effect of the drug in beagles. The modulatory action of ketamine was evident only at 1 and 4 min post bolus when the ketamine plasma concentrations ranged from 220 to 370 ng mL<sup>-1</sup> which is in the range reported to be analgesic in men (Clements & Nimmo 1981; Clements et al. 1982; Domino et al. 1982). Therefore it is not surprising that no modulation of the temporal summation occurred after T20 when the concentration for total ketamine in canine plasma ranged

between 50 and 100 ng mL<sup>-1</sup>, concentrations which are reported to be sub-analgesic in men (Clements & Nimmo 1981; Grant et al. 1981; Clements et al. 1982). Transitory psychomimetic side effects were seen after the loading bolus in all dogs as a moderate sedation (median score of 3.5 over 12) which unlikely affected the results of the electrophysiological tests.

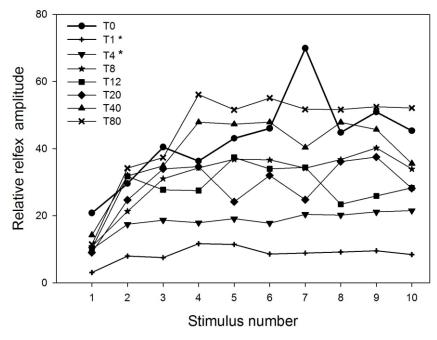


Figure 13. Median values showing the effect of ketamine on the temporal summation curves compared to baseline (T0). The repeated stimulations (10 stimuli, 5 Hz during 2 s) were given at temporal summation threshold intensity. \* Values of p (significance set at p < 0.05) derived via a Dunn's post hoc test after a significative Friedman repeated-measure ANOVA (p < 0.01)

# 12. Conclusions and Future applications

In conclusion, the work presented in this PhD thesis has provided a new, non invasive, robust experimental model of nociception in conscious dogs and has established a "baseline" condition for using the model in clinical routine to study the antinociceptive activity of drugs or to quantify the excitability of the nervous system in individual canine patients.

Study I showed that the NWR can be evoked from the fore- and hind limbs in dogs. The positive correlation between the intensity of stimulation and amplitude of the reflex and between the intensity of stimulation and behavioral reaction score confirms the nociceptive origin of the NWR. The train-of-five stimulus paradigm can be used as a standard stimulus. Thus, assessment of the NWR is proposed as a neurophysiologic tool for quantifying nociception in dogs

In study II by applying repeated stimulations, temporal summation was evoked. Temporal summation appeared to be more easily elicited from the hind limb, compared with the forelimb, but the reason for this difference remains to be elucidated. The 5-Hz frequency is recommended as the standard for future

studies in dogs. The evaluation of the temporal summation-evoked reflexes may be used to give information about changes in nociceptive system gain when analgesics are administered.

In study III, the stability of the NWR thresholds was demonstrated for the first time. A low-dose acepromazine exerted a mild tranquillization lasting 30 minutes without affecting NWR and TS thresholds, reflex characteristics, behavioural responses and supraspinal control after single and repeated stimulations. These findings suggest that acepromazine is deprived of antinociceptive action in dogs. Intravenous 0.01 mg kg<sup>-1</sup> acepromazine can facilitate the recordings in anxious dogs in clinical practice without altering the validity of this model.

In study IV, temporal summation was used for the first time to evaluate quantitatively the analgesic efficacy of a low-dose ketamine CRI in conscious dogs. Ketamine reduced considerably temporal summation. However its antinociceptive action was short lived most likely due to the low plasma level obtained, therefore we cannot recommend this low-dose ketamine CRI regimen as sole analgesic in dogs. Further research to find a CRI regimen for dogs resulting in stable antinociceptive plasma levels with minimal side effects should be undertaken.

There are many interesting future implementation possibilities based on the basic work presented in this thesis, i.e. to confirm the modular organization of the withdrawal reflexes in dogs and to investigate the effect of sex on the NWR and its characteristics.

By evaluating the modulating effects on NWR and temporal summation in an experimental setting, it will be possible to bring evidence of species-specific antinociceptive efficacy of different drugs,. Based on the results of study III and the upcoming pharmacokinetic study, we plan to find a ketamine CRI regimen resulting in stable antinociceptive plasma levels in dogs with minimal psychomimetic side effects. The modulatory effects on NWR and temporal summation of buprenorphine, a partial  $\mu$  agonist, could be studied too. Buprenorphine may represent a new therapeutic options for dogs affected of neuropathic and neoplastic pain requiring long term analgesic treatment, as it appears to dampen central sensitization (Kress; Penza et al. 2007). Another drug worthy investigating is tropisetron (5-hydroxytryptamine-3 receptor antagonist), which acts at spinal level and modulate central sensitization of dorsal horn neurons. The final goal would be for the benefit of the canine patients by offering better treatment strategies for central hypersensitivity especially for dogs not responding to conventional analgesics.

In humans, there is ongoing research to use the NWR and temporal summation as objective tools to detect and quantify central hyperexcitability in individual patients (Desmeules et al. 2003; Banic et al. 2004; Curatolo et al. 2004). In the same way, it is foreseen to implement the NWR and temporal summation model after acepromazine sedation in clinical routine as tools to detect and quantify the degree of sensory dysfunction in dogs affected from chronic malignant or non malignant pathologies (Hielm-Björkman et al. 2003; Beckman 2006). Furthermore this neurophysiologic model could be employed to assess objectively the efficacy of antinociceptive treatments in individual canine patients which would finally improve in the therapeutic strategies in dogs. To our knowledge, no investigation on this subject has been performed in dogs.

## 13. Tables

 Table 1. Evoked behavioral responses score

Score	Single stimulation	Repeated stimulation		
0	No movement	No movement		
1	Slight flexion of carpus/tarsus	Muscle twitch		
2	Flexion of elbow/stifle joint	Flexion of elbow/stifle joint followed by		
		relaxation		
3	Brisk flexion of elbow/stifle joint	Flexion of entire limb followed by relaxation		
4	Brisk flexion of the limb and flexion maintained	Flexion of limb, and flexion maintained		
5	Brisk flexion of the limb and general awareness (ie,	Sustained flexion of limb and general		
	turning the head toward the stimulated limb or	awareness (ie, turning the head toward the		
	attempts to stand from a lying position)	stimulated limb or attempts to stand from a		
		lying position)		
6	Brisk flexion of the limb, general awareness and	Sustained limb flexion, general awareness, and		
	vocalization	vocalization.		

**Table 2.** Incidence and characteristics (latency and relative amplitude) of the late reflex activity recorded in the 100 to 400 ms epoch for each muscle. Data are median (25-75% IQR).

 RMS: root-mean-square. -: no reflex activity. NA: not available

		Single pulse Stimulus			T	Train-of-five pulses stimulus		
Muscle	Intensity	Onset (ms)	Termination (ms)	Relative amplitude (RMS)	Onset (ms)	Termination (ms)	Relative amplitude (RMS)	
	$1 \mathrm{X} \mathrm{I}_{\mathrm{t}}$	-	-	-	-	-	-	
	1.2 X I <sub>t</sub>	-	-	-	-	-	-	
Cleidobrachialis	$1.5 \mathrm{X} \mathrm{I}_{\mathrm{t}}$	-	-	-	-	-	-	
	$2 \ge I_t$	-	-	-	-	-	29.8 (26.0-36.7)	
	3 X I <sub>t</sub>	-	-	-	NA	NA	NA	
	1 X I <sub>t</sub>	-	-	-	-	-	-	
	$1.2 \ \mathrm{X} \ \mathrm{I_t}$	-	-	-	-	-	-	
Deltoideus	$1.5 \mathrm{X} \mathrm{I}_{\mathrm{t}}$	-	-	-	110.6 (110.6-110.6)	146.8 (146.8-146.8)	52.6 (52.6- 52.6)	
	$2 \ \mathrm{X} \ \mathrm{I_t}$	-	-	-	107.6 (106.0-110.6)	146.8 (129.2-157.5)	14.9 (10.3-70.8)	
	3 X I <sub>t</sub>	-	-	-	NA	NA	NA	
	1 X I <sub>t</sub>	-	-	-	-	-	38.6 (38.6-38.6)	
	$1.2 \ \mathrm{X} \ \mathrm{I_t}$	-	-	-	119.1 (113.5-124.7)	165.5 (131.1-200.0)	13.93 (9.3-36.3)	
Biceps femoris	1.5 X I <sub>t</sub>	125.75 (102.7-148.8)	144.8 (122.3-167.3)	16.3 (10.0-22.5)	110.5 (104.7-116.4)	148.2 (131.1-165.4)	50.0 (18.9-45.5)	
	2 X I <sub>t</sub>	130.4 (102.4-158.5)	159.0 (122.3-195.7)	14.1 (10.8-17.3)	96.4 (87.1-105.7)	137.9 (127.2-148.7)	37.7 (10-114.7)	
	3 X I <sub>t</sub>	138.0 (120.4-155.6)	170.2 (151.7-188.8)	26 (20.2-31.8)	NA	NA	NA	
	1 X I <sub>t</sub>	-	-	-	-	-	34.7 (34.7-34.7)	
Tibialis anterior	$1.2 \ \mathrm{X} \ \mathrm{I_t}$	-	-	-	119.4 (103.7-174.4)	138.9 (129.9-152.6)	24.8 (6.3-75.0)	
	1.5 X I <sub>t</sub>	103.7(103.7-103.7)	167.3 (167.3-167.3)	26.0 (26.0-26.0)	122.4 (103.7-129.2)	154.6 (138.0-174.2)	26.0 (9.4-68.7)*	
	$2 \ge I_t$	106.5 (103.7-109.6)	150.1 (138.5-161.4)	23.4 (12.9-34.0)	109.1 (100.8-118.4)	144.3 (87.9-128.2)	66.4 (23.0-176.4)*	
	3 X I <sub>t</sub>	98.8 (96.0-103.7)	153.6 (140.9-161.4)	38.1 (23.7-39.7)	NA	NA	NA	

**Table 3**. Composite sedation score. The sedation score (0 to 12; no sedation to deep sedation) was assigned by adding up the ranking of different descriptors

	Consciousness	Eye	Responsiveness	Relaxation
0	Awake	Not rotated	Responds to voice	Moves spontaneously
1	Aware	Moderate rotation	Responds to touch	Relaxed, no shivering
2	Not aware but arousable	Rotated	Do not respond to touch	Very relaxed
3	Not aware, not arousable	Nystagmus	Hyperexcitable	Muscle tonus

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